

# Optical coherence tomography

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## Outline

- Part I:
  - Introduction to optical coherence tomography (OCT).
- Part II:
  - Modeling the light propagation in the OCT geometry.
- Part III:
  - Biomedical applications,
  - Extracting optical properties.

# Introduction to optical coherence tomography (OCT)

## Part I



### Outline – Part I

- Physical principle behind OCT
  - based on interference,
  - tomography comes about by scanning.
- Components and systems

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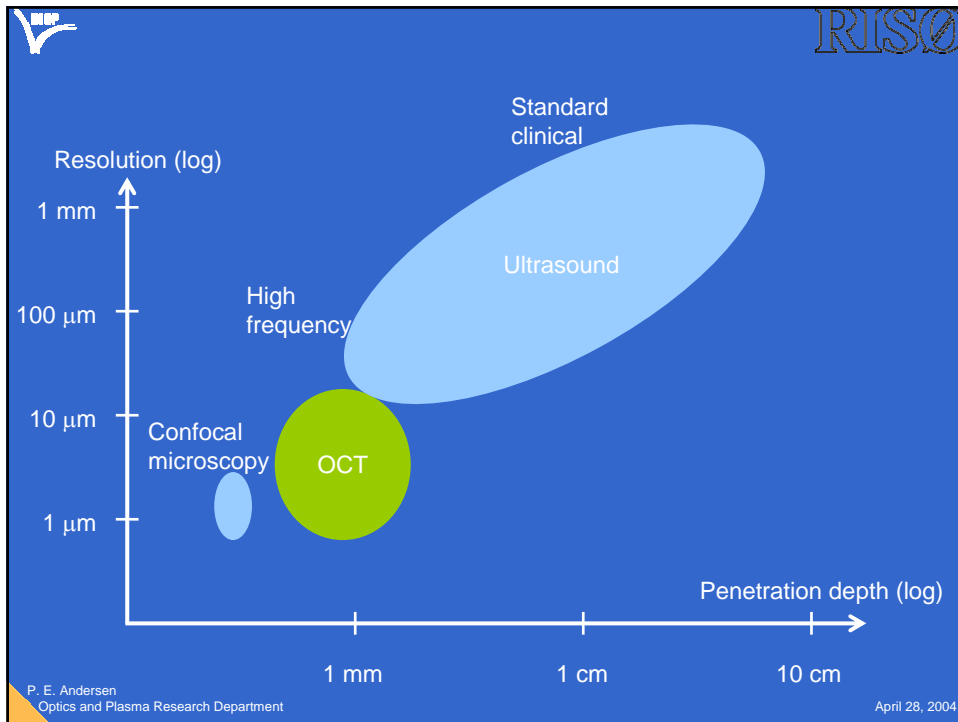
## Optical biopsy – definition

- The in situ imaging of tissue microstructure with a resolution approaching that of histology, but without the need for tissue excision and processing



## Optical coherence tomography

- Three-dimensional imaging technique with ultrahigh spatial resolution even in highly scattering media
- Based on measurements of the reflected light from tissue discontinuities
  - e.g. the epidermis-dermis junction.
- Based on interferometry
  - involves interference between the reflected light and the reference beam.

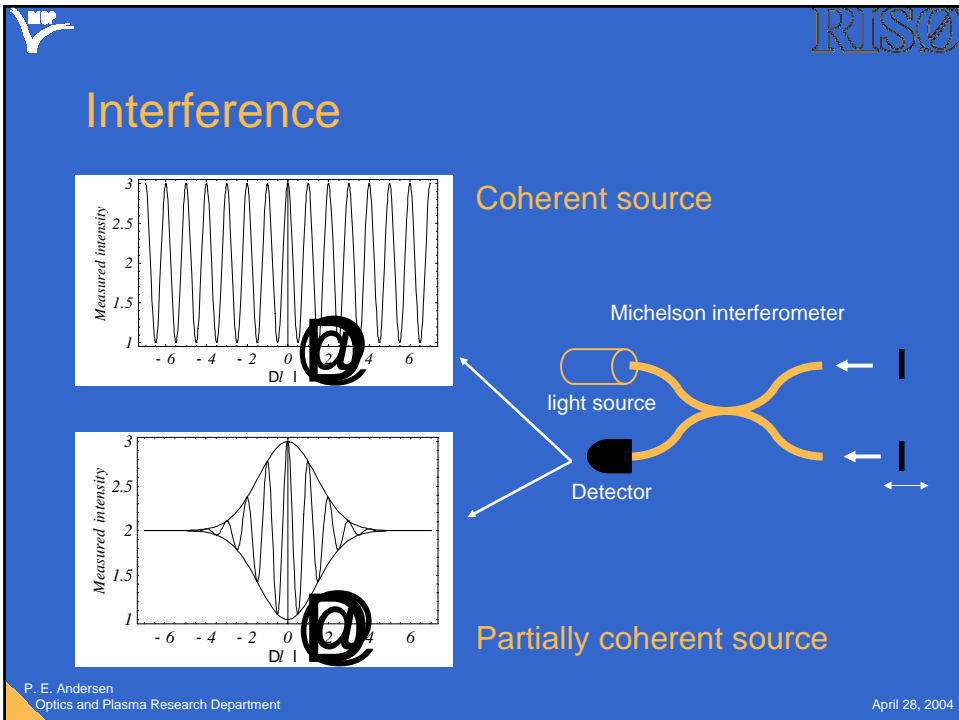
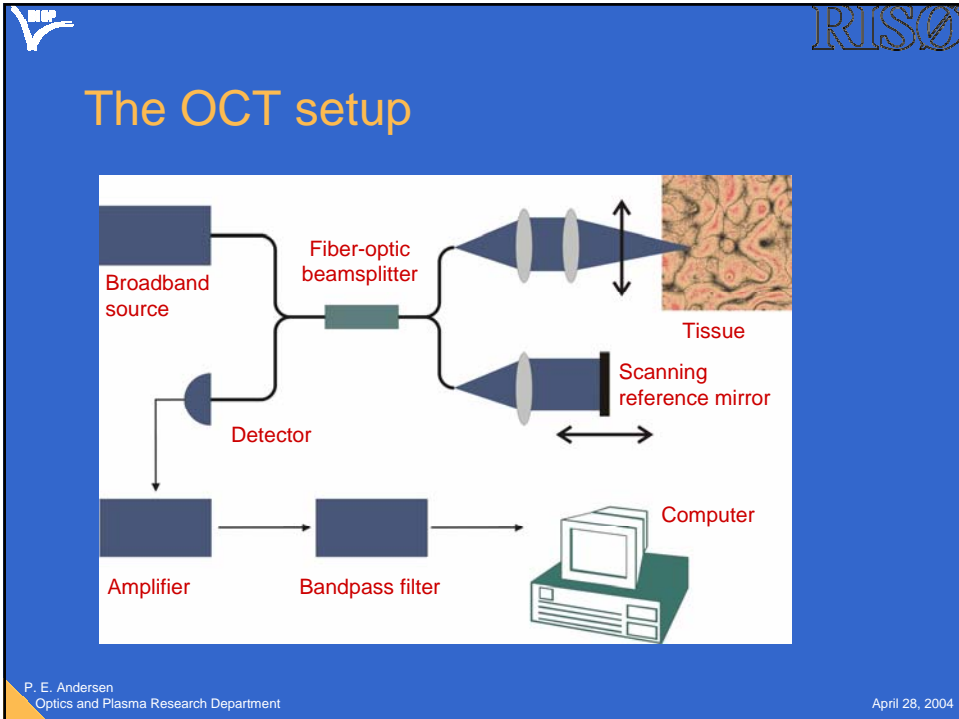


## OCT in non-invasive diagnostics

- Ophthalmology
  - diagnosing retinal diseases.
- Dermatology
  - skin diseases,
  - early detection of skin cancers.
- Cardio-vascular diseases
  - vulnerable plaque detection.
- Endoscopy (fiber-optic devices)
  - gastrology,
  - ...
- Functional imaging
  - Doppler OCT,
  - spectroscopic OCT,
  - optical properties,
  - PS-OCT.
- Guided surgery
  - delicate procedures
    - » brain surgery,
    - » knee surgery,
    - » ...

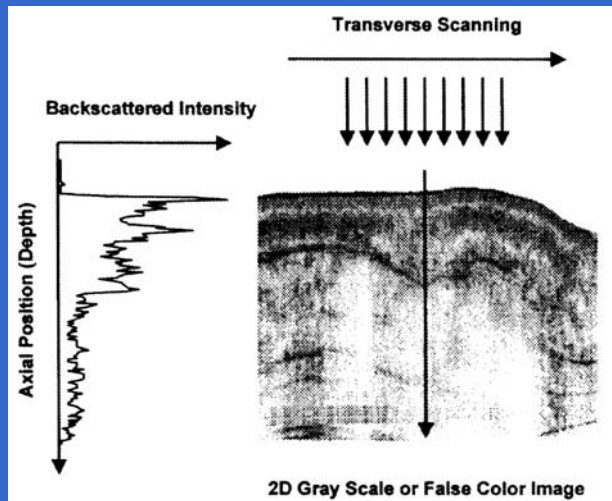
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## Construction of image

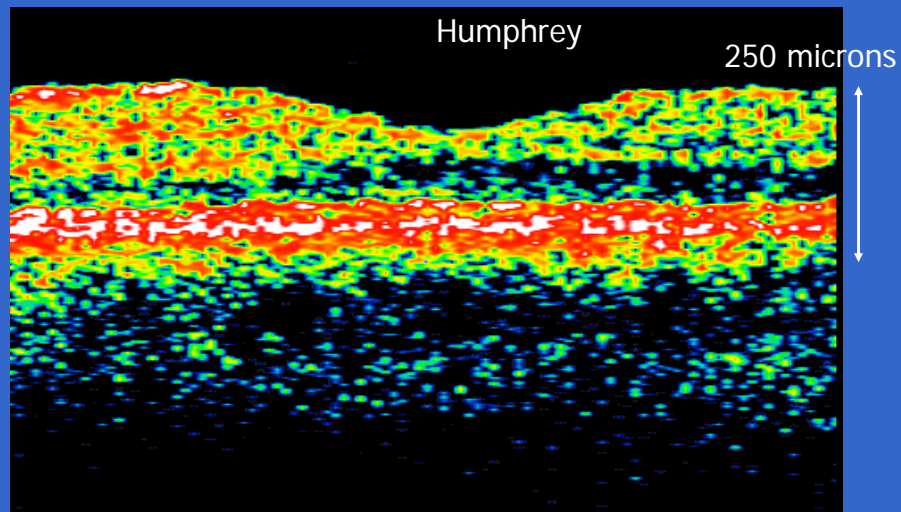


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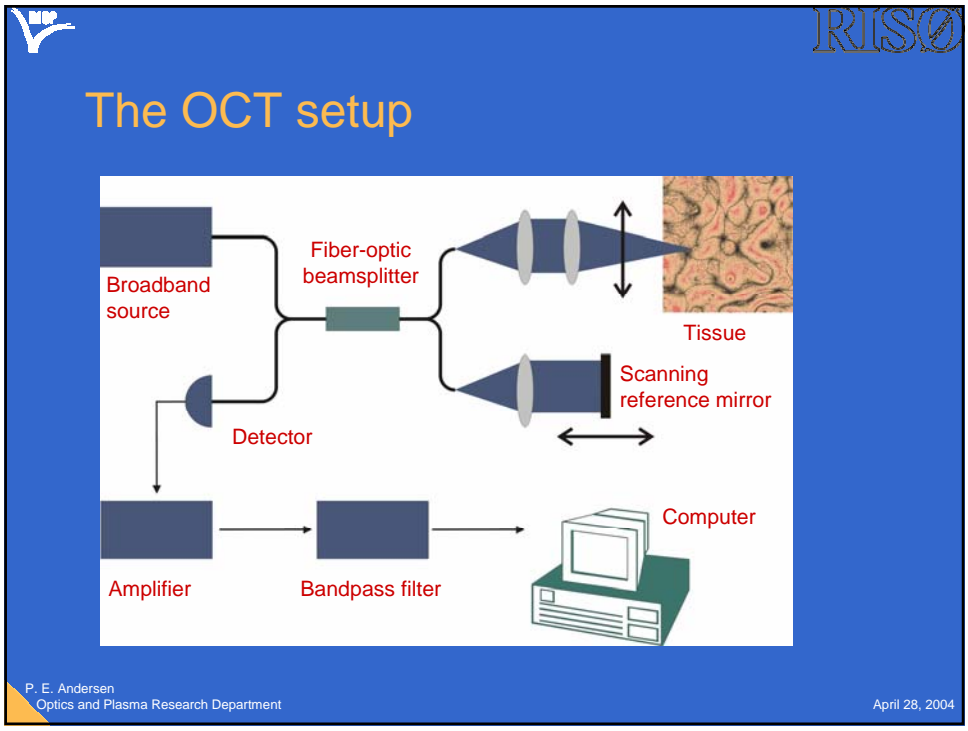
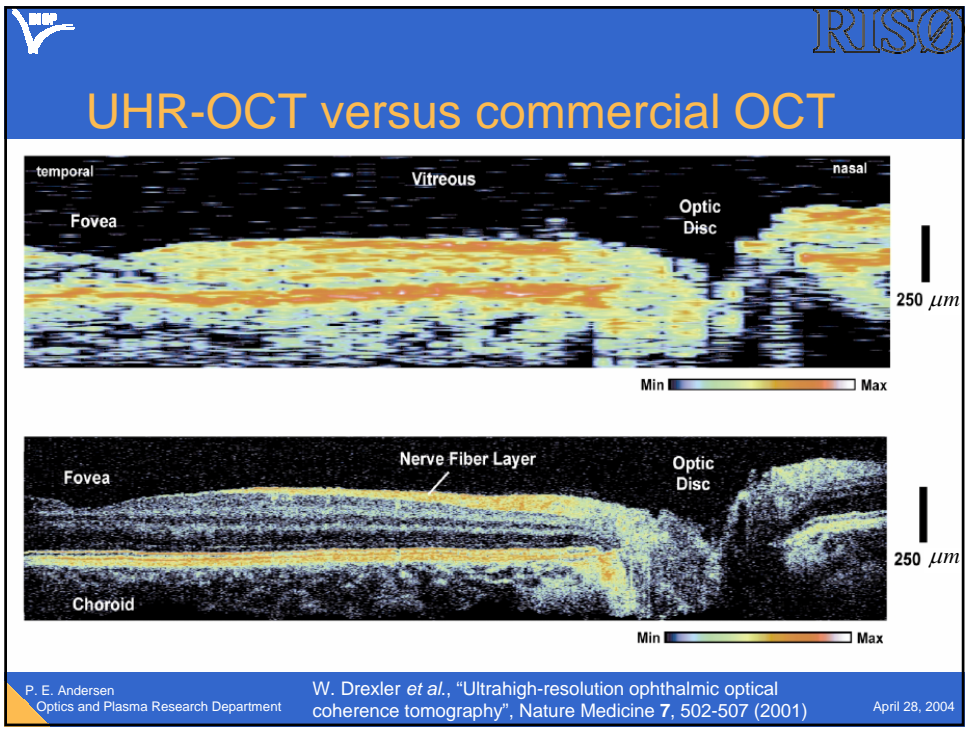
## Normal Eye

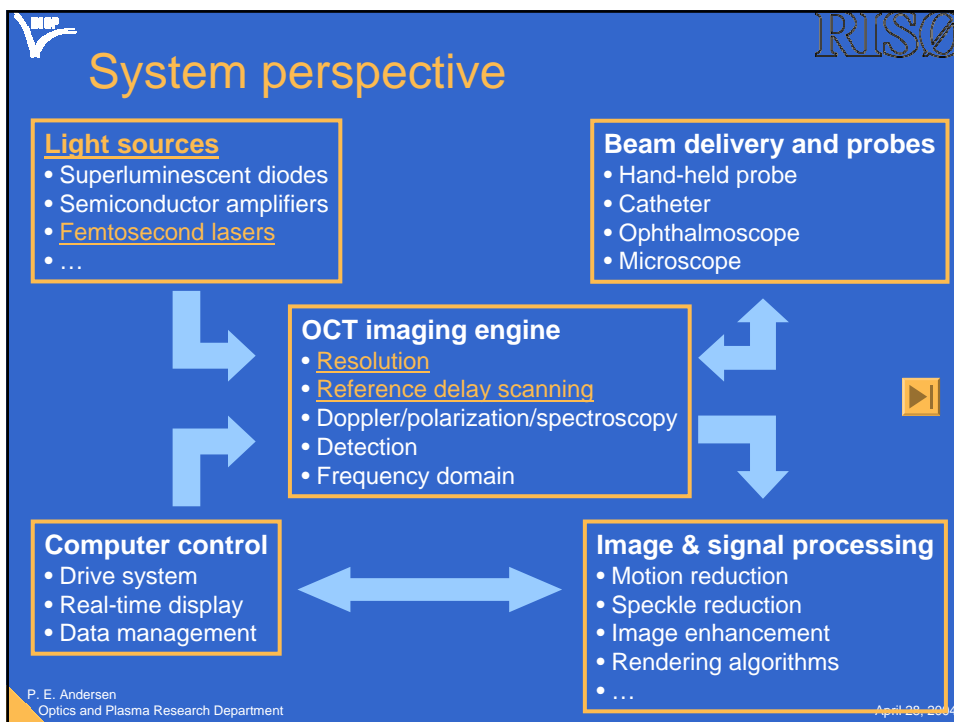


Nominal width of scan: 2.8 mm

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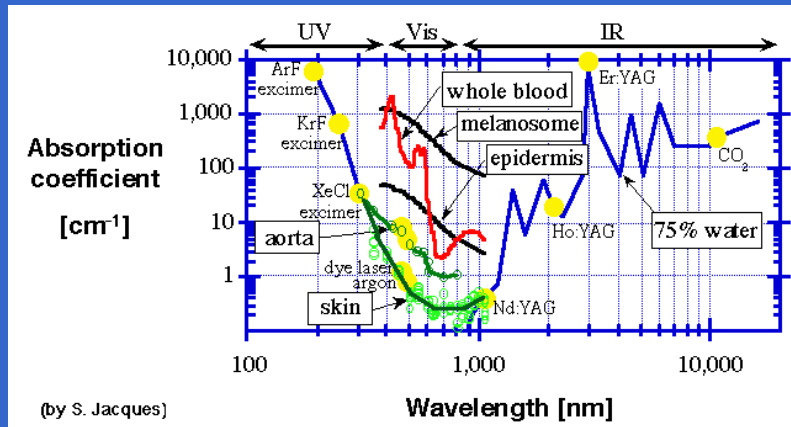




- 
- Choosing the light source**
- Four primary considerations
    - wavelength,
    - bandwidth,
    - power (in a single-transverse-mode),
    - stability;
      - » portability, ease-of-use, etc.
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- April 28, 2004

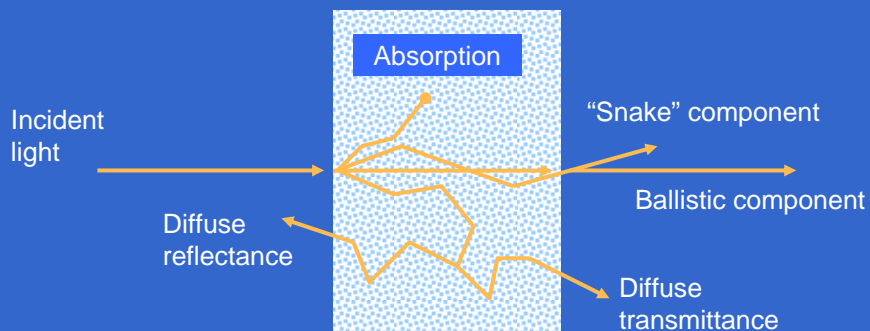


## Choose light source – wavelength

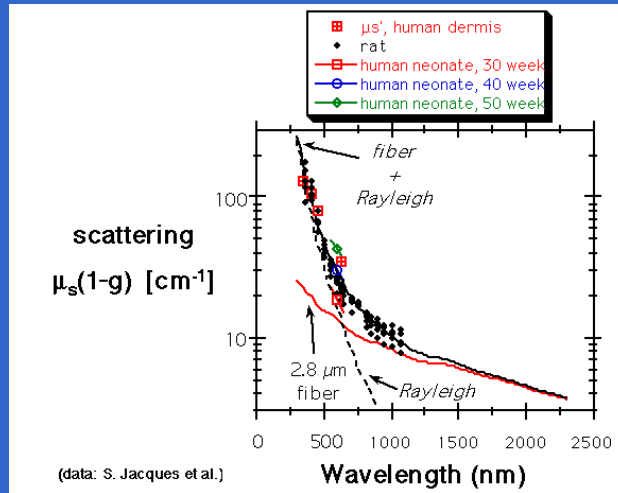


## Choose light source – wavelength

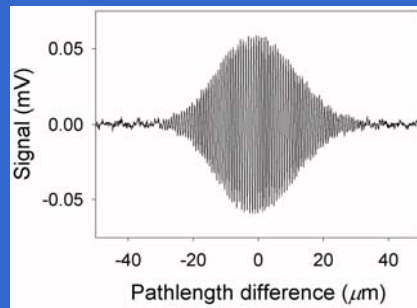
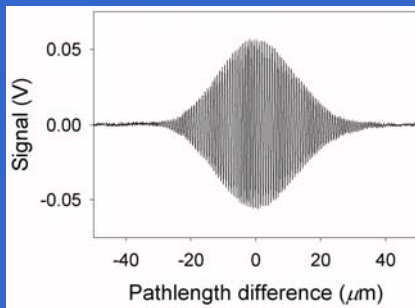
- Light propagation (Monte Carlo simulation)



## Choose light source – wavelength



## Raw signals



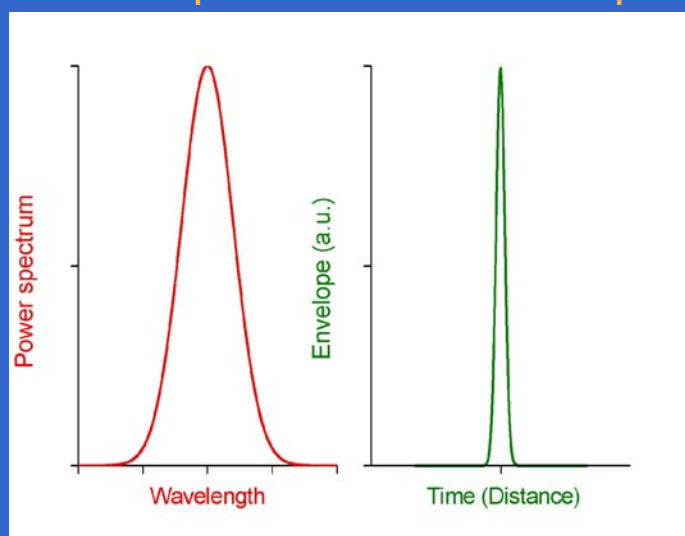


## Light source spectrum

- Basic property
  - the temporal coherence envelope function  $G(\tau)$  is related to the power spectral function  $S(\nu)$  through
$$G(\tau) = \text{FT}\{S(\nu)\}$$
    - » Wiener-Kinchine theorem
  - broadband source  $\leftrightarrow$  high axial resolution



## Source spectrum and envelope



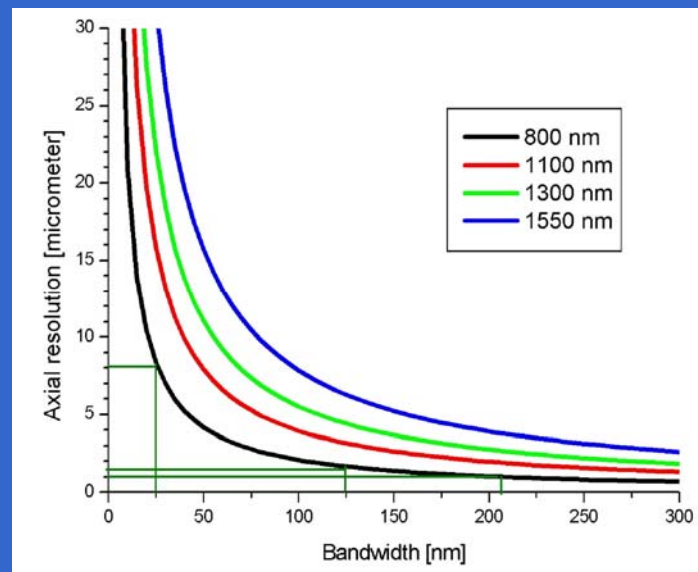


## Axial resolution

- The axial resolution is

$$l_c = \frac{2c \ln 2}{\rho} \frac{1}{Dn} = \frac{2 \ln 2}{\rho} \frac{l_0^2}{Dl} \gg 0.44 \frac{l_0^2}{Dl}$$

— notice that  $\Delta\lambda$  is the 3dB-bandwidth!





## Light sources for OCT (1/2)

- Continuous sources
  - SLD/LED/superfluorescent fibers,
  - center wavelength;
    - » 800 nm (SLD),
    - » 1300 nm (SLD, LED),
    - » 1550 nm, (LED, fiber),
    - » power: 1 to 10 mW (c.w.) is sufficient,
  - coherence length;
    - » 10 to 15  $\mu\text{m}$  (typically),
- Example
  - 25 nm bandwidth @ 800 nm  $\Rightarrow$  12  $\mu\text{m}$  coherence length (in air).



## Light sources for OCT (2/2)

- Pulsed lasers
  - mode-locked  $\text{Ti:Al}_2\text{O}_3$  (800 nm),
  - 3 micron axial resolution (or less).
- Scanning sources
  - tune narrow-width wavelength over entire spectrum,
  - resolution similar to other sources,
  - advantage that reference arm is not scanned,
  - advantage that fast scanning is feasible.



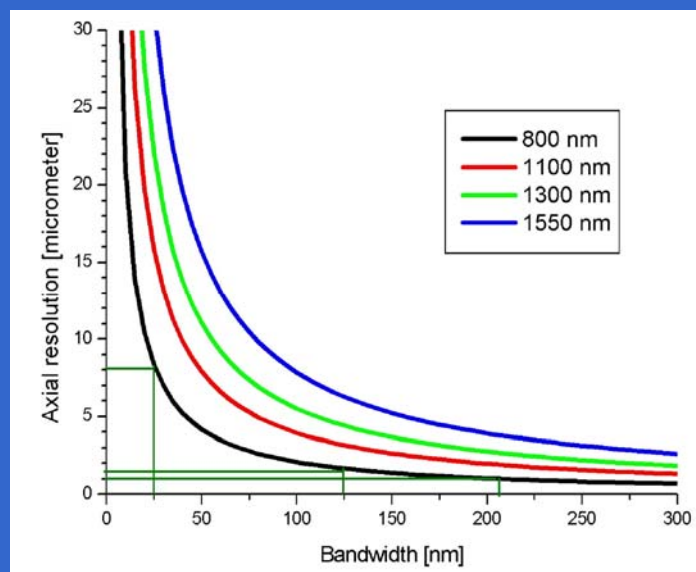
## OCT spatial resolution

- Axial and lateral resolutions are decoupled
- The axial resolution is

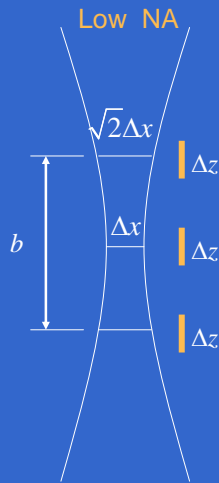
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— notice that  $\Delta\lambda$  is the 3dB-bandwidth!

- The lateral resolution is determined by the focusing conditions
  - optics
  - dynamic vs. static focusing



## Lateral resolution (1/2)

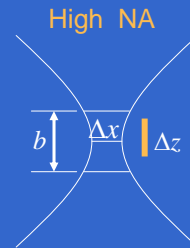


Lateral resolution

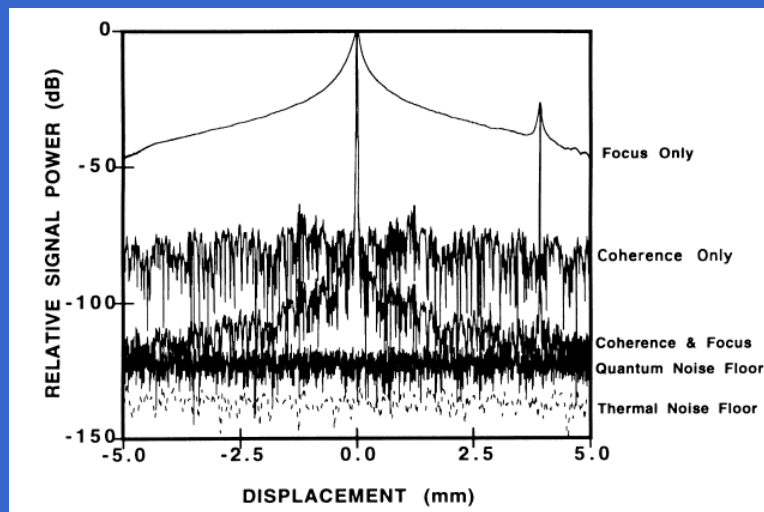
$$\Delta x = \frac{4\lambda}{\pi} \left( \frac{f}{d} \right)$$

Depth of focus

$$b = 2z_R = \pi \frac{\Delta x^2}{2\lambda}$$



## Lateral resolution (2/2)





## Ultra-high resolution OCT

- Broad bandwidth sources
  - solid-state lasers,
  - sub-5 fs pulse;
    - » Ti:Al<sub>2</sub>O<sub>3</sub> (Spectral bandwidth: 350 nm demonstrated),
  - other lasers/wavelengths available or needed.
- Special interferometers and fiber optics
  - support for broad spectral range,
  - dispersion balanced,
  - current system used for OCT: 260 nm bandwidth, ~1.5 $\mu$ m resolution.
- Chromatically corrected optics
  - aberrations can decrease resolution and SNR.
- Broad bandwidth detectors and electronics
  - dual balance detection,
  - low noise circuitry necessary.



## Scanning devices

- Piezo or motorized scanning devices
  - ideal for both longitudinal and lateral scanning.
- Galvanic mirrors
- Resonance scanners
- Helical mirrors
  - longitudinal scanning.
- Fiber stretcher
  - longitudinal scanning.

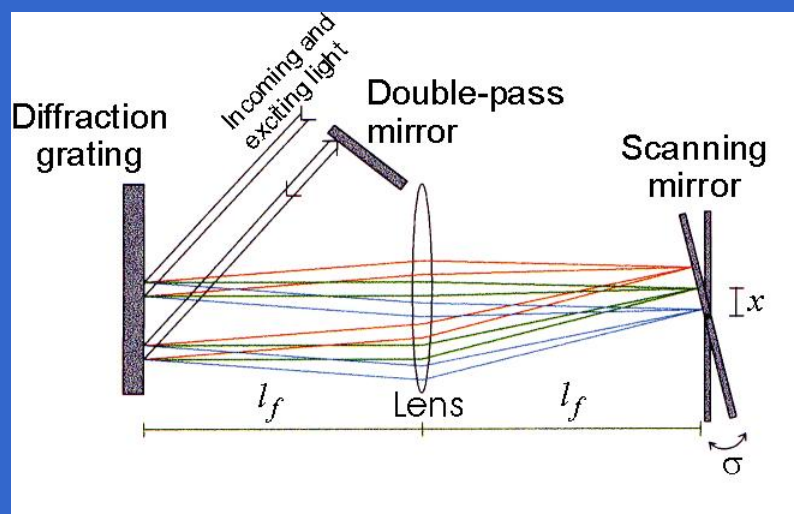


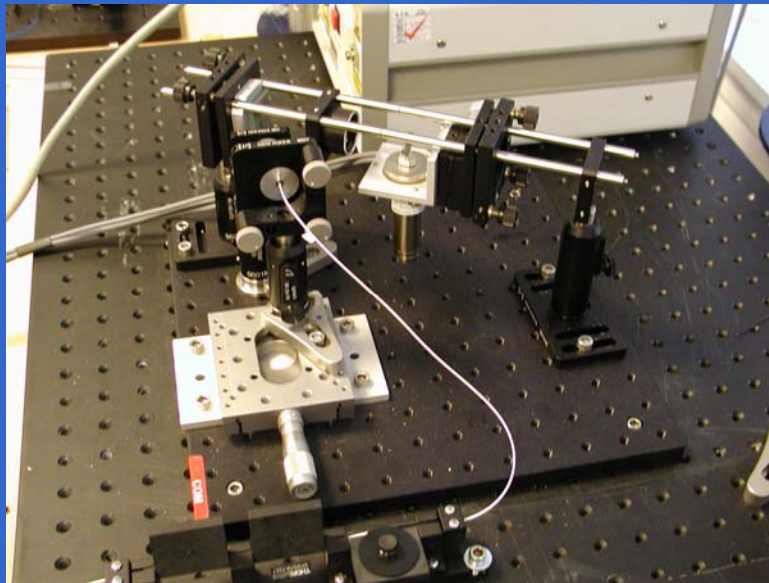
## Fourier domain rapid scanning optical delay line (RSOD)

- The technique was originally developed for femtosecond pulse measurements
  - based on Fourier-transform pulse shaping techniques.
- Relies on the basic property of the Fourier transform
  - phase ramp in the Fourier domain corresponds to a group delay in the time domain.

$$x(t - t_0) \xleftrightarrow{\mathfrak{F}} X(\omega) \exp\{-j\omega t_0\}$$

## RSOD setup





## RSOD characteristics

- Free-space group pathlength
- Bandwidth

$$\Delta l_g = 4\sigma x - \frac{4\sigma l_f \lambda_0}{p}$$

- $p$ : the grating pitch,
- $f$ : focal length,
- $\sigma$ : mirror angle.

$$\Delta f = \frac{2\Delta\lambda}{\lambda_0^2} \left( 2x - \frac{2l_f \lambda_0}{p} \right) \frac{\partial \sigma}{\partial t}$$

- Interferogram central frequency

$$f_0 = \frac{4x}{\lambda_0} \frac{\partial \sigma}{\partial t}$$



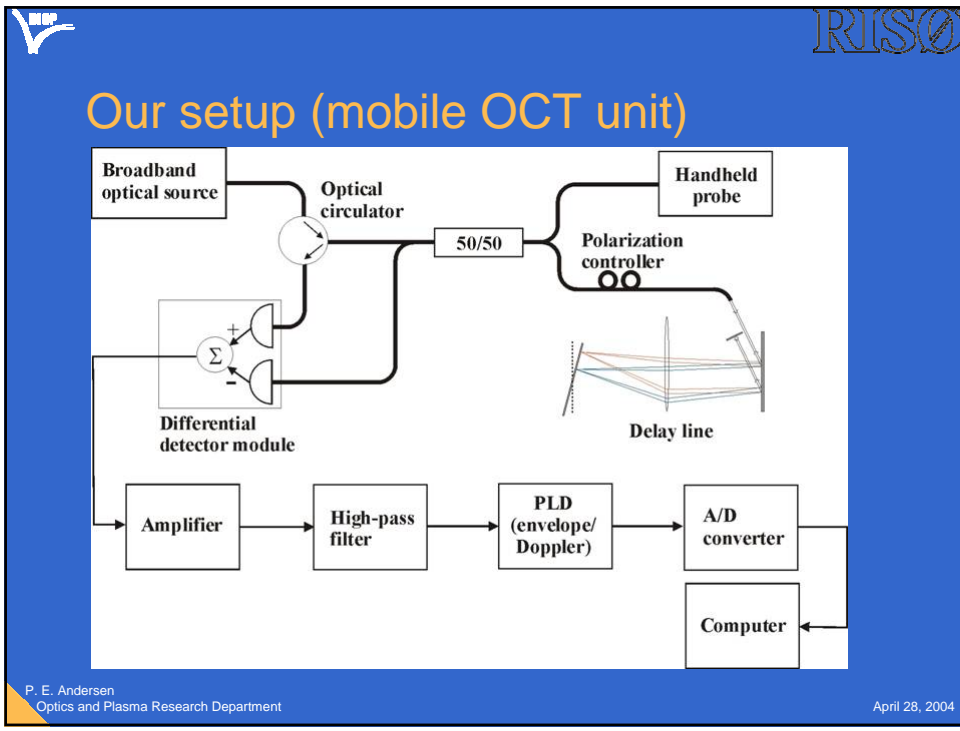
## RSOD – figures-of-merit

- Scanning capabilities (galvo)
  - ~ 200 Hz,
  - ~ 5 mm.
- Scanning capabilities (resonant)
  - ~ 4-8 kHz,
  - ~ 5 mm.
- Advantages
  - dispersion compensation feasible since phase and group delays may be separated,
  - center frequency of interferogram is adjusted through axial position.



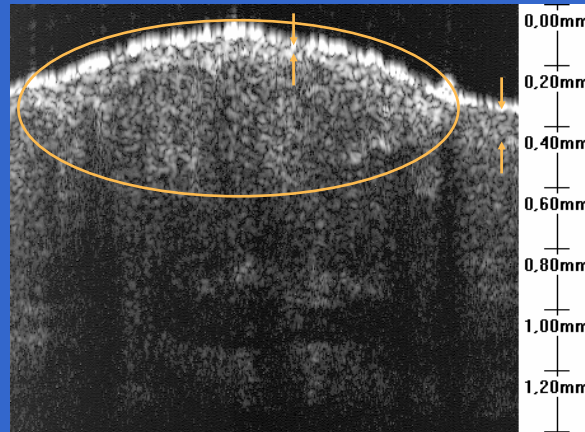
## Light propagation in sample

- The sample
  - need to describe light-tissue interaction taking temporal and spatial coherence properties into account;
    - » can transport theory be used?
- Light-tissue interaction to be modelled using the extended Huygens-Fresnel principle
  - Part II of this lecture,
  - correlation between tissue, state of tissue (lesions) and optical properties?
    - » Part III of this lecture.



## BCC II

- Layers
- Thinning of layers



## OCT: Figures-of-merit – summary

- Dynamic range
  - 100 dB (or better).
- Resolution (typical)
  - 1-10 micrometers.
- Penetration depth
  - depending on wavelength/tissue,
    - » 1-2 mm (typically) for 1300 in skin tissue.
- Axial and lateral resolutions are decoupled
  - important for applications.
- Pixel density is related to spatial resolution and image acquisition time
  - $N_z = 2 * L_z / dz$ ,
  - $N_x = 2 * L_x / dx$ ,
  - image acq. time:  $T = N_x * f_s$ ,
  - scan velocity:  $v_s = L_z * f_s$ .
- Image acquisition
  - seconds or less,
  - real-time OCT.
- Clinical adaptation
  - interfaced to standard equipment,
  - fiber-optic devices,
  - endoscopes.



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